

1 Normal kinematics of the upper cervical spine during the Flexion-Rotation Test –
2 in vivo measurements using Magnetic Resonance Imaging

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Abstract

26 The Flexion-Rotation Test (FRT) is proposed to assess mobility primarily at
27 C1-C2. However, there is no in vivo measurement investigating the validity of the
28 FRT. The purpose of this study was to investigate the validity of the FRT by
29 evaluating kinematics of the upper cervical spine during the FRT using MRI. A
30 secondary purpose was to examine measurement reliability. Nineteen
31 asymptomatic female subjects (mean age: 22.2 years) were evaluated with a
32 0.2-T horizontally open MRI unit. The segmental rotation angles from
33 Occiput-C1 to C3-C4 and the C4 vertebra were assessed with the head
34 maximally rotated to both the right and the left in two conditions – neck in neutral
35 and in flexion. A repeated measures ANOVA revealed an interaction between the
36 two different neck starting positions and segment levels ($P < 0.0001$). Post-hoc
37 analysis revealed that there were significant reductions in the flexed position
38 ($P < 0.0001$) except for at Occiput-C1. While there was only a 16.3% reduction
39 in rotation range at C1-C2, the reduction was 68.1% at C2-C3, 61.4% at
40 C3-C4, and 76.9% at segments below C4, respectively. The inter- and intra-
41 observer measurement reliability were substantial. These results support the
42 validity of the FRT as a clinical measure of atlanto-axial mobility.

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Keywords

45 In vivo, MRI, Segmental rotation, Upper cervical spine

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Introduction

49 Restriction of range of motion appears to be a generic feature of neck pain
50 disorders, and it is routinely assessed in the clinical evaluation of patients
51 (Dall'Alba et al., 2001; Woodhouse and Vasseljen, 2008). Clinical examination of
52 primary plane movements provides overall information about movement of the
53 spinal segments collectively, but some tests reportedly are biased toward a
54 certain cervical segment (Edwards, 1992; Dvorak et al., 2008).

55 The Flexion-Rotation Test (FRT) described by Dvorak et al (1998) is
56 commonly used as an assessment of mobility in the upper cervical region. The
57 cervical spine is placed in end-range flexion, in an attempt to block rotation of all
58 vertebrae below C2. It is postulated that rotation in end-range cervical flexion
59 occurs predominantly at the atlantoaxial joint (C1-C2) (Hall and Robinson, 2004;
60 Ogince et al., 2007; Dvorak et al., 2008; Hall et al., 2008b). Proponents of this
61 test report its relative ease of use with minimal practitioner skill required (Hall et
62 al., 2008b), which is in contrast to other passive segmental mobility tests (Jull et
63 al., 1988; Jull et al., 1997). Normal range of motion is approximately 45° to both
64 sides (Hall and Robinson, 2004; Hall et al., 2008b). Range of motion less than
65 33° to one side is rated as abnormal (Ogince et al., 2007; Hall et al., 2008b). In
66 addition, range of motion recorded during the FRT is stable over time (Hall et al.,
67 2010b). Hence, the FRT has been used clinically in cervicogenic headache
68 diagnosis and as a treatment outcome measure after physical therapy
69 interventions to the upper cervical spine (Hall et al., 2007; Hall et al., 2008a; Hall
70 et al., 2010a). However, to date there has been no in vivo study to measure
71 cervical segmental movements during the FRT to confirm the validity of the FRT.

72 The purpose of this study was two-fold. The first purpose was to investigate

73 the validity of the FRT as a test of predominantly C1-C2 motion. This was
74 achieved by measuring and comparing segmental rotation from Occiput-C1 to
75 C3-C4 and rotation of the C4 vertebra, which indicates total rotation of segments
76 distal to C4, with the neck in neutral position and in flexion position, using
77 Magnetic Resonance Imaging (MRI). The second purpose was to examine
78 measurement reliability of rotation angles derived from MRI data.

79

80 Materials and Methods

81 Participants

82 Subjects were volunteers recruited from advertising in the Sapporo Medical
83 University. Forty-five asymptomatic subjects who were less than 145cm tall,
84 without any history of significant cervical spine or shoulder girdle disorders were
85 included. Twenty-two subjects were immediately excluded as they could not
86 achieve end-range cervical flexion in the narrow space within the MRI unit. To
87 identify potential cervical spine disorders, all remaining volunteer subjects were
88 screened by sagittal T2-weighted and axial T2*-weighted MRI of the neck and by
89 a routine physical examination of range of motion of the neck and upper limbs.
90 Two orthopedic surgeons experienced in MRI evaluations, inspected all MRI
91 images for abnormalities on the sagittal T2-weighted images (FSE, FOV: 250,
92 TR/TE: 2570/140msec, Thickness: 5.0mm, Interval: 6.0mm, Scan time 5:39) and
93 the axial T2*-weighted images (GE, FOV: 200, TR/TE: 900/20msec, Thickness:
94 5.0mm, Interval: 5.0mm, Scan time 5:24). Four subjects were found to have
95 potential evidence of musculoskeletal disorders (non-symptomatic disc bulging)
96 and were thus excluded. As a result, 19 females of the original 45 volunteer

97 subjects completed the study. The mean height of the 19 subjects was 141.2cm
98 (range, 136-145cm) and mean age 22.2 years (range, 19-27 years).

99 All subjects were informed of the study design and the procedures to be
100 used and all provided informed consent prior to data collection. Data collection
101 was conducted in the Shinoro Orthopedic, Sapporo, Japan. Approval for this
102 study was granted by the Society of Physical Therapy Science.

103

104 Measurement method

105 *Equipment*

106 MRI of the cervical spine was performed with a 0.2-T horizontally open unit
107 (AIRISmate, HITACHI Inc., Sapporo, Japan). The participants were placed in the
108 supine position on a custom-made positioning device that was designed and
109 constructed to fit into the MRI unit and attach to the examination table. It was
110 located beneath the flexible receiver surface coil (MR-JCL-72 separate type,
111 HITACHI Inc. Sapporo, Japan) and used to guide the movements of neck
112 rotation from neck in neutral position and end-range flexion position. Both
113 shoulders and chest were fixed firmly by belts (Figure 1).

114

115 *Data acquisition method*

116 The range of vertebral rotation was assessed at each level from the occiput
117 to the C4 vertebra under two conditions: head rotation with the neck in neutral
118 position (lying without a pillow) and in a flexed position. The angle of the spinal
119 column in the sagittal plane in the neutral and flexed positions was measured
120 and calculated from the angle of bisection of the lines drawn parallel to the

121 inferior end-plates of the C2 and C7 vertebra. This measurement has previously
122 been shown to be reliable (Takasaki et al., 2009a). It was described as positive if
123 it rotated anteriorly relative to the line described by C7, from sagittal T1-weighted
124 images (GE, FOV: 250, TR/TE: 90/12msec, Thickness: 5.0mm, Interval: 9.0mm,
125 Scan time 0:35). The sagittal T1-weighted image was captured before the
126 measurements of head rotation in each neck position.

127 For each measurement of the vertebral rotations (neutral and in flexion), an
128 examiner passively maintained the end-range head rotated position during
129 scanning. The order of testing (neck in neutral or in flexion) was randomized
130 between subjects.

131

132 *Measurement angles*

133 Segmental rotation angles (Occiput-C1, C1-C2, C2-C3 and C3-C4) were
134 calculated from the vertebral rotation angles as follows. Firstly, each vertebral
135 rotation from the occiput to C4 vertebra was measured from axial T1-weighted
136 images (GE, FOV: 260, TR/TE: 450/15msec, Thickness: 2.5mm, Interval: 2.5mm,
137 Scan time 2:56). Rotation of the occiput was measured by drawing a line from
138 the midpoint of the foramen magnum to the nasal septum on the T1-weighted
139 axial image (Figure 2) and defining the rotation value between that line and
140 sagittal plane (vertical image frame). The rotations of C1 and C2 were defined
141 using a line drawn through the lateral masses of the atlas dividing C1
142 symmetrically into anterior and posterior parts (Figure 3), and a line drawn
143 parallel to the posterior border of the body of C2 (Figure 4). The rotation values
144 of the C1 and C2 vertebrae were defined between those lines and coronal plane

145 (horizontal image frame). The angles of the C3 and C4 vertebrae were defined
146 using a line drawn from the midpoint of each spinous process to the center of
147 each vertebral body (Figure 5). The sagittal plane (vertical image frame) was
148 used as a reference. Secondly, segmental rotation angles were calculated by
149 subtracting the rotation values of the lower vertebrae from those of the upper
150 vertebrae. Each measurement was taken on two occasions and for analysis and
151 presentation of results, the averaged values of two measurements were used. In
152 addition, the angles of rotation to the left and right at each segment were
153 summed.

154 To examine inter- and intra-observer variation of the measurement of the
155 segmental rotations and the C4 vertebral rotation, two examiners experienced in
156 the measurement of MRI data were included. The two different examiners, blind
157 to each other's assessment, measured the same series to study inter-observer
158 variation. To investigate intra-observer variation, one of the two examiners
159 measured the images twice on two separate occasions. On the second occasion,
160 the examiner was blind to the results of the first measurement session.

161

162 *Statistics*

163 A repeated measures ANOVA was used to compare movement patterns of
164 the segmental rotation angles and the C4 vertebral rotations (combined rotation
165 from segments below the C4 vertebra) between the neutral position and the
166 flexed position. The Shapiro-Wilk's test was used to examine for normal
167 distribution of data and post-hoc analysis employed paired t-tests and/or
168 Mann-Whitney U tests to examine mean differences of segmental rotations and

169 the C4 vertebral rotations between the two neck starting positions. Statistical
170 analysis was performed using SPSS version 18.0 (SPSS Inc., Tokyo, Japan).
171 Statistical significance was set at $P < 0.05$.

172 The intraclass correlation coefficients (ICC) were calculated with the use of
173 $ICC_{(1,1)}$ and $ICC_{(2,1)}$ to examine inter- and intra-observer accuracy of MRI data
174 measurements and to estimate the minimum number of measurement
175 repetitions to achieve good measurement repeatability ($ICC > 0.8$). The standard
176 error of measurement (SEM) of the segmental rotation angles from Occiput-C1
177 to C3-C4 and C4 rotation was also calculated for each investigator to examine
178 measurement accuracy of MRI data.

179

180

Results

181 The total ranges of head rotation in the neutral and flexed positions were
182 $163.0^\circ \pm 8.3^\circ$ and $88.4^\circ \pm 7.6^\circ$, respectively. The mean sagittal angles of the
183 cervical spinal column when the head was rotated in the neutral and flexed
184 positions were $-3.3^\circ \pm 3.5^\circ$ and $52.4^\circ \pm 10.8^\circ$, respectively.

185 Preparatory analysis confirmed that the data for Occiput-C1, C1-C2, and
186 C3-C4 were normally distributed. Mean segmental rotation angles (left and right
187 summed) at each cervical motion segment in each neck position (neutral and
188 flexion) are presented in Table 1. Notably, the range of rotation at the C1-C2 level
189 was 51.9% of total head rotation in the neutral position and 73.5% of available
190 range in the flexed position. A repeated measures ANOVA revealed an
191 interaction between the two different neck starting positions and segment levels
192 ($P < 0.0001$). Post-hoc analysis revealed that except for the Occiput-C1 segment,

193 there were significant reductions ($P < 0.0001$) in the segmental rotation ranges
194 with the neck in flexion compared with the neutral neck position.

195 The intra- and inter-observer-ICC and the SEM of the vertebral rotation
196 angles are shown in Table 2. Substantial intra- and inter-observer reliability of
197 the measures was demonstrated and the magnitude of measurement error was
198 low. Based on the results of the $ICC_{(1,1)}$, it was determined that the average value
199 of two measurements, rather than a single measurement, provided higher levels
200 of repeatability ($ICC > 0.8$).

201

202

Discussion

203 This study supports the validity of the FRT, described by Dvorak et al (1998),
204 as a test which predominately tests rotation of the atlanto-axial joint. In
205 considering the distribution of segmental rotation between the neutral and flexed
206 neck positions, the segmental rotation between the occiput and C1 was
207 negligible in both test positions, which is consistent with the known kinematics of
208 this motion segment (Bogduk and Mercer, 2000). At the atlanto-axial joint, there
209 was a 16.3% reduction in range of rotation in the flexed compared to the neutral
210 position, but this was minimal compared to the reduction which occurred at the
211 other cervical segments: 68.1% at C2-C3, 61.4% at C3-C4 and 76.9%
212 collectively at the cervical segments distal to C4. Thus, flexing the cervical joints
213 and pre-tensioning the posterior cervical articular and other soft tissues in the
214 neck flexion position has an apparent greater effect on the segments distal to
215 C1-C2. The 16.3% reduction in C1-C2 motion measured in this study might
216 reflect changes in tension of the soft tissue structures local to this joint including

217 the alar ligaments and tectorial membrane in the FRT (Crisco et al., 1991; Oda et
218 al., 1992). The C1-C2 segment provided 73.5% of the total rotation in the flexed
219 position. This lends supports to the validity of the FRT as an assessment of
220 predominantly atlanto-axial joint rotation.

221 To our knowledge this is the first study to measure segmental range of
222 cervical rotation during the FRT. All previous reports that have investigated the
223 FRT have used external measurement devices. In the present study, the total
224 range of head rotation in the FRT position was $88.4^{\circ} \pm 7.6^{\circ}$. Walmsley et al
225 (1996) and Amiri et al (2003) used an external electromagnetic device, the
226 3Space Tracker system, and reported ranges of $100.8^{\circ} \pm 12.9^{\circ}$ and $81.1^{\circ} \pm 10.3^{\circ}$
227 respectively for total head rotation in the FRT position. Hall et al (2008b) used a
228 Cervical Range of Motion goniometer and recorded 89° of rotation in the FRT.
229 The small differences between our and other studies likely arise from different
230 measurement methods as well as different FRT procedures (Walmsley et al.,
231 1996; Amiri et al., 2003) but the comparability between the MRI and external
232 measures supports the latter's use for a clinical evaluation.

233 MRI is a highly accurate means of measuring rotation range that has been
234 used extensively in other kinematic studies of the cervical spine (Karhu et al.,
235 1999; Gradl et al., 2005; Ishii et al., 2006; Takasaki et al., 2009b). Despite the
236 number of studies to have used MRI to investigate cervical rotation range, ours
237 is the first to report the reliability and measurement error for this technique. We
238 found good levels of inter- and intra-observer reliability for the measurement
239 technique. ICCs were greater than 0.7, with narrow 95% confidence interval
240 values for mean range of rotation. Furthermore the largest standard error of

241 measurement was only 0.4°. Hence the ranges reported in our study can be
242 interpreted with a reasonable level of confidence.

243 The present study had two potential limitations. Firstly, the study included
244 only a small number of subjects and all were female (because of the height
245 restriction to fit in the narrow space of the MRI unit), young and healthy without
246 cervical spine disorders. Nevertheless, Walmsley et al (1996) found no
247 significant differences between genders for head rotation from a cervical neutral
248 or maximally flexed position, but there were significant differences with age.
249 Therefore, our angular data cannot be extrapolated to older subjects and further
250 study of this age group is required. The second limitation was that segmental
251 movement of the lower cervical segments was not assessed because of
252 technical limitations. Further studies are required to assess rotation at all cervical
253 segments during the FRT.

254

255

Conclusion

256 MRI is a reliable and accurate method of measuring cervical segmental
257 rotation. Head rotation when the neck is in a flexed position occurs primarily at
258 the atlanto-axial joint whereas rotation is markedly restricted at all other cervical
259 motion segments. These data lend support to the FRT as a valid clinical test of
260 atlanto-axial mobility. There can be some confidence that the predominant
261 location of the restriction is at the atlanto-axial joint when side to side differences
262 of rotation are found in the FRT in the clinical assessment of patients with
263 cervical disorders.

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